High Deborah Number Flows Through 3D Contractions at the Microscale

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ABSTRACT

In this work, we report a rich sequence of elastic transitions captured experimentally using a viscoelastic, shear-thinning solution. The experiments were carried out in a microchannel with a sudden contraction followed by a smooth expansion, taking advantage of the distinctive conditions provided by microfluidic viscoelastic flows, i.e., the capability of achieving high Deborah numbers (De) while keeping the Reynolds numbers low enough so that inertia does not have a significant impact. We studied the effect of De on the flow patterns and were able to achieve a flow regime, at sufficiently high De, in which the flow becomes unsteady with the main vortices formed upstream of the contraction varying in size substantially and very rapidly resembling what Afonso et al. [1] coined as the back-shedding regime. This process is accompanied by the formation of secondary vortices, which are shed in the upstream flow direction. A similar phenomenon was also captured by our preliminary numerical simulations performed using the Oldroyd-B constitutive equation.

Keywords: viscoelastic fluids, contraction flow, elastic instabilities, flow visualization, finite volume method

1 INTRODUCTION

The flow through sudden contractions is a long-standing problem and has been reported in numerous experimental and numerical works, using both Newtonian and non-Newtonian fluids (cf. [1-9]). There are three main types of configuration used in sudden contraction flow research: axisymmetric, planar 2-D and planar 3-D geometries. The latter are especially relevant at the microscale as many microfabrication techniques yield planar channels of constant depth where wall effects are non-negligible.

In spite of the simple geometry, these flows exhibit complex flow patterns comprising regions of strong shearing close to the walls and nonhomogeneous extension along the centerline near the contraction region [10]. One of the remarkable features of viscoelastic fluid entry flows is the formation and subsequent enhancement of vortices upstream of the contraction plane.

As a consequence of miniaturization, contraction flows at the microscale occur under low Reynolds number (Re) conditions corresponding to the laminar flow regime [6,7,10]. Furthermore, the small length-scales and large contraction ratios typical of microfluidics result in high extensional deformation rates and high total extensional strains that typically lead to strong nonlinear flow effects even with dilute and semidilute polymer solutions [6,7,11]. In particular, Rodd et al. [6,7] have studied experimentally the flow of various polyethylene oxide solutions through a 16:1 contraction and have shown a series of inertio-elastic transitions that could not have been observed in equivalent experiments at the macroscale.

In numerical terms, simulations of viscoelastic fluid flows through contractions are notoriously difficult at high Deborah numbers (De) and are usually limited to flows below a critical De. Above the critical De value, the numerical simulations typically present mesh dependency problems (even with refined meshes) and are often not able to obtain a converged solution. Very recently, Afonso et al. [1] used a finite volume method with the log-conformation formulation, originally proposed by Fattal and Kupferman [12] that allowed reliable numerical simulations to be extended to much higher Deborah numbers than in previous works. The results of their 2D simulations using the Oldroyd-B constitutive equation, showed that local flow unsteadiness appears at a relatively low Deborah number (De = 2.5) and that a subsequent increase in De leads a growth of the flow unsteadiness resulting in asymmetric flow with alternate back-shedding of vorticity from pulsating upstream recirculating eddies. Additionally, the authors report a frequency doubling mechanism, which eventually leads to a chaotic regime at high De. These numerical results were the motivation for our own experimental work reported here, in which we aim to capture experimentally the same type of flow features and try to understand, aided by numerical simulations, the mechanisms underlying the flow transitions that take place at high Deborah numbers.

2 EXPERIMENTAL METHODS

2.1 Microchannel Geometry and Set-up

The experiments were carried out using microfabricated channels consisting of a sudden contraction followed by a smooth expansion with a nearly-hyperbolic shape.
geometry is symmetric about the plane $y = 0$ and was fabricated in polydimethylsiloxane, PDMS (Sylgard 184, Dow Corning), from an SU-8 photoresist mold by standard soft-lithography techniques. The geometry produced is planar with a constant depth $h = 45 \mu m$ and is depicted in Fig. 1, where the main variables are identified.

The width of the inlet and outlet channels ($W_i$) is the same and equal to 400 $\mu m$ and the expansion region is well defined by the equation:

$$y = \pm 200 [1 + 0.05 (L' - x) - 2.5 \times 10^{-5} (L' - x)^2]$$  \hspace{1cm} (1)$$

valid for $0 \leq x \leq L'$ with $L' = 123 \mu m$. The contraction ratio defined as $CR = W_i/W_2$, where $W_2$ is the projected channel width at the contraction plane, amounts to $CR = 6.4$ for the present geometry.

A syringe pump (Harvard Apparatus PHD2000) was used to control the flow rate at the inlet using syringes with different volumes according to the required flow rate. For the flow visualizations, we used an optical set-up composed of an inverted epi-fluorescence microscope (DMI 5000M, Leica Microsystems GmbH) fitted with an appropriate filter cube (Leica Microsystems GmbH, excitation BP 530–545 nm, dichroic mirror 565 nm, barrier filter 610–675 nm). The flow patterns were captured by streak photography (with long exposures) using a CCD camera (Leica Microsystems GmbH, DFC350 FX), and a 100W mercury lamp as illumination source. For this purpose, the fluid was seeded with 1 $\mu m$ fluorescent tracer particles (Nile Red, Molecular Probes, Invitrogen, Ex/Em: 520/580 nm).

All images shown in this work were captured at the center plane of the geometry using a 20$\times$ (NA = 0.25) microscope objective (Leica Microsystems GmbH). For the set-up used, the depth of field corresponds to $\delta z = 4.55 \mu m$ calculated according to:

$$\delta z = \frac{n\lambda_0}{(NA)^2} \times \frac{ne}{(NA)M}$$  \hspace{1cm} (1)$$

where $n$ is the refractive index, $\lambda_0$ is the wavelength of the light (in vacuum), NA is the numerical aperture of the objective, $e$ is the minimum detectable size and M is the total magnification (in this case $e/M = 0.65 \mu m$).

### 2.2 Fluid Rheology

The viscoelastic fluid used in the experiments is a solution of polyethylene oxide (PEO, with a molecular weight $M_w = 8\times10^6$ g mol$^{-1}$ supplied by Sigma-Aldrich) in a water/glycerol mixture prepared using a magnetic stirrer at low speeds, in order to prevent unnecessary mechanical degradation of the polymer molecules. The composition (by weight) is 0.4% PEO, 66.3% water and 33.3% glycerol.

The fluids were characterized rheologically using a rotational rheometer (Anton Paar, Physica MCR301) and capillary break-up extensional rheometer (Haake CaBER 1, Thermo Scientific). The latter is employed to quantify the response of the fluid to an extensional deformation. In particular, a liquid bridge confined between the two plates (of diameter $D_p = 6$ mm) is stretched as the top plate moves ($-50 \text{ ms} \leq t \leq 0$) from an initial ($h_i = 3$ mm) to a final height ($h_f = 12$ mm) and the subsequent evolution of the filament diameter is monitored using a laser micrometer. In the regime when surface tension and elasticity govern the filament drainage the local extensional rate in the filament is constant and the diameter of the filament ($D$) decays exponentially with time ($t$) according to [13]:

$$D(t)/D_p \propto \exp[-t/(3\lambda)]$$  \hspace{1cm} (2)$$

The filament thinning evolution of the PEO solution is shown in Fig. 2 and the fit of Equation (2) to the region of exponential decay is shown in red, yielding a relaxation time $\lambda = 123$ ms.

The steady-shear viscosity measurements were carried out at 20$^\circ$C for a range of shear rates ($1 \leq \dot{\gamma} / s^{-1} \leq 10000$) using a cone and plate geometry (50 mm in diameter and $1^\circ$ angle) and are shown in Fig. 3a. In Fig. 3b, we illustrated the storage and loss moduli ($G'$ and $G''$) in dynamic shear flow. The fluid exhibits a shear thinning behavior, as a result of shear induced changes in the microstructure - as

![Figure 1. Micrograph of the contraction geometry used in the experiments, where the shape of the quasi-hyperbolic walls are marked in red.](image1)

![Figure 2. Filament thinning obtained during a CaBER experiment (only part of the experimental data is plotted to improve visually the figure).](image2)
the shear rate is increased, the polymer molecules orient and align with the flow direction.

The shear viscosity, \( \eta \), increases with the shear rate, \( \dot{\gamma} \), due to the alignment of polymer molecules with the flow direction. This phenomenon is illustrated in Figure 3.

**3 NUMERICAL METHOD AND GOVERNING EQUATIONS**

The equations we need to solve are those of conservation of mass and momentum:

\[
\nabla \cdot \mathbf{u} = 0 \quad (3)
\]

\[
\rho \frac{\partial \mathbf{u}}{\partial t} + \rho \mathbf{u} \cdot \nabla \mathbf{u} = -\nabla p + \nabla \cdot \mathbf{\tau} + \eta \nabla^2 \mathbf{u} \quad (4)
\]

together with an appropriate constitutive equation for the extra stress tensor. Here we use the Oldroyd-B model:

\[
\mathbf{\tau} = \lambda \left( \frac{\partial \mathbf{u}}{\partial t} + \nabla \mathbf{u} + (\nabla \mathbf{u})^T \right) = \eta \left( \nabla \mathbf{u} + \nabla \mathbf{u}^T \right) + \lambda \left( \nabla \cdot \mathbf{u} + \nabla \mathbf{u}^T \cdot \mathbf{\tau} \right) \quad (5)
\]

A fully-implicit finite-volume method was used to solve Equations (3) – (6). The numerical technique has been described in detail elsewhere [14-16] and is not repeated here due to space restrictions.

**4 RESULTS AND DISCUSSION**

The effect of the Deborah number on the flow patterns captured experimentally was studied by varying the flow rate imposed using the syringe pump. For very low flow rates, the flow resembles that obtained under Newtonian creeping flow conditions (Fig. 4a), and an increase in the flow rate leads to the formation and growth of symmetric lip (Fig. 4b) and (later) corner vortices (Fig. 4c) upstream of the contraction as observed previously in sudden and smooth contractions with dilute polymer solutions [2]. This is followed by an asymmetric steady flow region, in which the two vortices exhibit slightly different sizes; eventually, as the flow rate is increased further, the flow becomes unsteady and the main vortices pulsate, growing and shrinking slightly in a periodic fashion (Fig. 4d). At sufficiently high Deborah numbers, this process becomes more dramatic and resembles what Afonso et al. [1] coined as back-shedding regime in which the size of the main vortices varies substantially and very rapidly (Fig. 4e), a process accompanied by the formation of upstream secondary vortices, which are shed in the upstream flow direction (Fig. 4e). This time dependent behavior including the formation and shedding of upstream secondary vortices was also captured by our numerical simulations with 2D meshes using the Oldroyd-B model (Fig. 5). Although the experimental and numerical results are not in quantitative agreement, the results are encouraging and we expect that using a more suitable constitutive equation (eg. PTT model) and 3D calculations will be able to provide more realistic predictions.

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**REFERENCES**


Figure 4. Effect of the flow rate on the flow patterns obtained experimentally. For $Q = 1.0 \text{ ml/h}$ the images were captured further upstream of the contraction and as such the contraction region is not visible. The white lines were drawn to indicate the boundary walls of the microchannel.